Neuromodulation of reinforced skill learning reveals the causal function of prefrontal cortex

Eran Dayan1 | Jasmine Herszage2 | Rony Laor-Maayany2 | Haggai Sharon3,4 | Nitzan Censor2

1Department of Radiology, Biomedical Research Imaging Center and Neuroscience Curriculum, University of North Carolina at Chapel Hill, Chapel Hill, North Carolina
2School of Psychological Sciences and Sagol School of Neuroscience, Tel Aviv University, Tel Aviv, Israel
3Center for Brain Functions and Institute of Pain Medicine, Tel Aviv Sourasky Medical Center, Tel Aviv, Israel
4Sackler Faculty of Medicine, Tel Aviv University, Tel Aviv, Israel

Correspondence
Nitzan Censor, Sharet Building, School of Psychological Sciences, Tel Aviv University, Tel Aviv 69978, Israel.
Email: censornitzan@post.tau.ac.il

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Abstract
Accumulating evidence has suggested functional interactions between prefrontal cortex (PFC) and dissociable large-scale networks. However, how these networks interact in the human brain to enable complex behaviors is not well-understood. Here, using a combination of behavioral, brain stimulation and neuroimaging paradigms, we tested the hypothesis that human PFC is required for successful reinforced skill formation. We additionally tested the extent to which PFC-dependent skill formation is related to intrinsic functional communication with this region. We report that inhibitory noninvasive transcranial magnetic stimulation over lateral PFC, a hub region with a diverse connectivity profile, causally modulated effective reinforcement-based motor skill acquisition. Furthermore, PFC-dependent skill formation was strongly related to the strength of functional connectivity between the PFC and regions in the sensorimotor network. These results point to the involvement of lateral PFC in the neural architecture that underlies the acquisition of complex skills, and suggest that, in relation to skill acquisition, this region may be involved in functional interactions with sensorimotor networks.

KEYWORDS
functional MRI, motor learning, prefrontal cortex, reward, sequence learning, transcranial magnetic stimulation

1 | INTRODUCTION

Multiple lines of evidence suggest that lateral prefrontal cortex (lPFC) may play a significant role in modulating diverse learning and memory systems (Cieslik et al., 2012; Hasan et al., 2013; Jarbo & Verstynen, 2015; Preston & Eichenbaum, 2013). The hippocampus and its extensive connections with the prefrontal cortex (Goldman-Rakic, Selemon, & Schwartz, 1984) have been suggested as the key circuitry necessary for declarative memory formation, while sensorimotor circuits have been linked to procedural memory formation (Dayan & Cohen, 2011; Doyon & Benali, 2005), both facilitated by reward mechanisms (Abe et al., 2011; Dayan, Hamann, Averbeck, & Cohen, 2014; Hamann, Dayan, Hummel, & Cohen, 2014; Miendlarzewska, Bavelier, & Schwartz, 2016). Altogether, accumulating evidence has pointed to functional interactions within large-scale learning and memory systems, involving IPFC (Cieslik et al., 2012; Hasan et al., 2013; Jarbo & Verstynen, 2015; Preston & Eichenbaum, 2013; Witt et al., 2008). However, a mechanistic account on how these systems interact in the human brain to enable motor behavior is missing, forming a gap in knowledge as to how motor skill memory is formed in ecologically relevant learning environments.

Here, we used a combination of noninvasive brain stimulation and functional MRI (fMRI) to study the causal role of human IPFC in formation of reinforced skill learning, and its functional relation to large-scale functional networks. Functional and/or structural connections exist between the IPFC and sensorimotor (Cieslik et al., 2012; Hasan et al., 2013), declarative/hippocampal (Preston & Eichenbaum, 2013), and reward systems (Haber, 2011; Jarbo & Verstynen, 2015). This region is among a set of densely inter-connected hub regions which are believed to play a key role in information integration within large-scale brain systems (van den Heuvel & Sporns, 2011). In addition, using different skill acquisition paradigms, previous studies have pointed to a relation between PFC and motor skill learning (Gomez Beldarrain, Gafman, Ruiz de Velasco, Pascual-Leone, & Garcia-Monco, 2002; Kamiński et al., 2013), suggesting that the degree of PFC involvement relies on the cognitive demands of the performed tasks (Robertson, Tormos, Maeda, & Pascual-Leone, 2001; Witt et al., 2008). We thus hypothesized that the
IPFC is causally involved in formation of reinforced skill learning, and as such, is related to connectivity in functional networks that interact with the IPFC. To address this hypothesis, we tested whether perturbing brain IPFC activity in a controlled manner, via repetitive transcranial magnetic stimulation (rTMS) (Robertson et al., 2001) would affect skill acquisition. We then tested the relation between the effects of stimulation and the strength of intrinsic functional connections with IPFC. We had subjects train on a skill learning task (Figure 1), where performance was reinforced with monetary reward. In half of the sessions, training took place immediately after inhibitory rTMS was applied to right IPFC, contralateral to the hand used in the skill learning task (consistent with previous studies, Pascual-Leone et al., 1996; Robertson et al., 2001). In the second half of the sessions, administered in a crossover design, training took place after stimulation of the vertex, a commonly used control site (Dafotakis et al., 2008; Dayan et al., 2013; Ko et al., 2008; Nowak et al., 2008). In the remaining subjects, the order was reversed, with the first training session administered right after vertex stimulation, and the second after IPFC stimulation. As in previous studies, subjects executed a sequential finger-tapping task with their left nondominant hand, to eliminate a possible ceiling effect on learning (Censor, Dimyan, & Cohen, 2010; Censor, Horovitz, & Cohen, 2014; Censor, Dimyan, & Cohen, 2014; de Beukelaar, Woolley, & Wenderoth, 2014; Korman et al., 2007; Walker, Brakefield, Allan Hobson, & Stickgold, 2003; Karni et al., 1998). During the task, subjects were required to repeatedly tap a 5-element sequence of finger movements as quickly and accurately as possible. Monetary reward was stochastically administered, as a strategy to facilitate learning gains (see Section 2).

### 2.1 Subjects

Twenty healthy volunteers (8 males and 12 females; mean age = 26.1 ± 0.8 years) participated in the study. Subjects were all right handed. Five additional subjects were excluded from the experiment: three subjects were excluded before receiving rTMS due artifacts in the MRI scans, and two subjects stopped their participation during the TMS session due to discomfort. All subjects provided written informed consent and all procedures were in accordance with a protocol approved by the Tel Aviv Sourasky Medical Center and Tel Aviv University’s Ethics committees. Musicians and video-gamers (past or present) were excluded from the study, as well as subjects with psychiatric or neurological history. In addition, subjects were required to sleep at least 6 hr before each of the experimental sessions.

### 2.2 Procedure and task

The study comprised three sessions, with the main (stimulation) sessions following a crossover design. Subjects first underwent an imaging session where resting-state scans were acquired, in which they were instructed to keep their eyes closed and not fall asleep. Then, subjects were randomized and performed two training sessions of the sequential finger-tapping task in a within-subject crossover design: half of the subjects performed a training session with one of the two sequences right after receiving rTMS to right IPFC (see more details below) and then returned 7 days later to perform the untrained sequence right after receiving rTMS to the vertex, as a control site (Dafotakis et al., 2008; Dayan et al., 2013; Ko et al., 2008; Nowak et al., 2008). In the remaining sessions, the order was reversed, with the first training session administered right after vertex stimulation, and the second after IPFC stimulation. As in previous studies, subjects executed a sequential finger-tapping task with their left nondominant hand, to eliminate a possible ceiling effect on learning (Censor, Dimyan, & Cohen, 2010; Censor, Horovitz, & Cohen, 2014; Censor, Dimyan, & Cohen, 2014; de Beukelaar, Woolley, & Wenderoth, 2014; Korman et al., 2007; Walker, Brakefield, Allan Hobson, & Stickgold, 2003; Karni et al., 1998). During the task, subjects were required to repeatedly tap a 5-element sequence of finger movements as quickly and accurately as possible (Censor et al., 2010; Karni et al., 1995, 1998) (Figure 1). The task included one 30 s baseline trial (before TMS, see below), and 12 additional trials (after TMS), lasting 30 s each, interleaved with 30 s breaks. Tapping movements were performed using a 4-key response box (Cedrus Lumina LU440) which was placed in front of the subjects at a comfortable distance and height. The order of sessions was counterbalanced across participants, to minimize carry-over effects, and different sequences were used in each session (4-1-3-2-4 and 4-2-3-1-4), to minimize carry-over effects. “4,” “3,” “2,” and “1” corresponded to the index, middle, ring, and little fingers, respectively. In each training session, half of the trials were rewarded, in which subjects could win 1 Shekel per every five correct sequences (3.5 Shekels roughly equal 1 USD). Prior to each rewarded trial the instructions on the screen explicitly indicated that in the next trial subjects could win 1 Israeli Shekel for every five
correct sequences they tapped. A short (5 s) feedback phase was provided after each rewarded trial indicating how much money they have won in the trial (for instance if the subject tapped 22 sequences she/he was given a "You won 4 Shekels" feedback). Rewarded and unrewarded trials were stochastically administered, as a strategy to facilitate learning gains (Dayan, Averbeck, Richmond, & Cohen, 2014; Dayan, Hamann, et al., 2014), limiting the presentation of consecutive rewarded or unrewarded trials to not more than two in succession. Response data were collected for offline analysis using Psychtoolbox (MATLAB 8.4). During each trial, the sequence was displayed at the middle of the screen and remained in this position throughout the trial. The number of correct sequences tapped during each trial served as our primary behavioral outcome measure, a common and highly replicable end-point measure in sequence learning (Censor et al., 2010; Censor, Dayan, et al., 2014; Censor, Horovitz, et al., 2014; de Beukelaar et al., 2014; Karni et al., 1995; Korman et al., 2007; Walker et al., 2003).

### 2.3 Noninvasive brain stimulation

On each of the two experimental sessions, the main task (12 trials) was performed immediately following application of rTMS at 1 Hz for 15 min, delivered to either lPFC or the vertex as a control site (Dafotakis et al., 2008; Dayan et al., 2013; Ko et al., 2008; Nowak et al., 2008). Of note, rTMS over the vertex has been a reliable control condition, as the auditory and somatosensory activations caused by vertex TMS are similar to those of real TMS (Sandrini, Cappa, Rossi, Rossini, & Miniussi, 2003; Sandrini, Censor, Mishoe, & Cohen, 2013; Sandrini, Umlità, & Rusconi, 2011). LPFC was localized based on the international 10–20 system for EEG electrode placement. Based on studies (Griškova, Rukšėnas, Dapšys, Herpertz, & Höppner, 2007; Herwig, Satripi, & Schönfeldt-Lecuona, 2003) locating the IPFC at the F3 electrode placement, we used the homolog F4 location, to target the IPFC contralateral to the nondominant hand performing the behavioral task. This approach has been common for PFC stimulation (Rossi et al., 2001; Sandrini et al., 2003, 2013). Following the identification of the stimulation target, a neuro-navigation system (Brainsight 2, Rogue Research, Montreal, Canada, www.rogue-research.com) was used to maintain coil stability. In addition, the neuro-navigation system was used to coregister participants’ heads and to mark stimulation sites prior to rTMS administration. Four landmarks were used for coregistering the participants head to their MRI anatomic scan (nasion, tip of the nose, left and right crus of helix).

Stimulation was given at 100% of resting motor threshold measured over the same hemisphere, for 15 min, at a frequency of 1 Hz, a common protocol that has been shown to affect cortical excitability beyond the duration of the TMS application itself (Chen et al., 1997; Sandrini et al., 2011), and more specifically applied for PFC offline stimulation (Sandrini et al., 2013). With this common protocol, we could expect the decrease in cortical excitability to last at least 15 min post stimulation (Chen et al., 1997). The resting motor threshold was defined as the minimal primary motor cortex (M1) stimulation intensity yielding 5 out of 10 motor-evoked potentials (MEPs) greater than 0.05 mV in the left first dorsal interosseous (FDI) muscle (Rossini et al., 1994).

### 2.4 Behavioral data analysis

Behavioral data were analyzed with SPSS 23. A standard behavioral outcome measure was used, the number of correct sequences per trial, which accounts for both speed and accuracy (Censor et al., 2010; Censor, Dayan, et al., 2014; de Beukelaar et al., 2014; Korman et al., 2007; Walker et al., 2003). Learning gains were then measured as the difference between performance at baseline and peak performance at the last three trials of the session (Censor et al., 2010; Censor, Horovitz, et al., 2014; de Beukelaar et al., 2014; Walker et al., 2003). Paired t-tests were used to test for between session differences in baseline performance, and for differences in stimulation-dependent learning gains in rewarded and unrewarded trials. Finally, we tested stimulation-dependent differences in learning gains using a repeated measures Analysis of Variance (ANOVA) with stimulation type (IPFC vs. control) and performance (baseline vs. peak) as within-subjects factors.

### 2.5 Imaging data acquisition

Imaging data were acquired with a 3 T Siemens Magnetom Prisma scanner equipped with a 20-channel head coil at the Wohl Institute for Advanced Imaging, Tel Aviv Sourasky Medical Center. Structural images were acquired with an MPRAGE sequence (repetition time/echo time [TR/TE] = 1860/2.74 ms; flip angle = 8°; field of view [FOV] = 256 × 256 mm; slice thickness = 1 mm; 208 axial slices). Resting state fMRI images were acquired with a gradient echo-planar imaging (EPI) sequence of functional T2*-weighted images (TR/TE = 2000/35 ms; flip angle = 90°; FOV = 384 × 384 mm; slice thickness = 4 mm; 34 interleaved axial slices per volume). The functional scans comprised a total of 240 volumes which lasted 8 min. The first three volumes were discarded to account of T1-equilibrium effects. Two subjects (of the total 20) were scanned with different functional parameters (TR/TE = 3000/35 ms; flip angle = 90°; FOV = 672 × 672 mm; slice thickness = 3 mm; 46 interleaved axial slices per volume). We confirmed that all imaging results were retained when excluding these two subjects.

### 2.6 Imaging data analysis

Imaging data analysis was based on SPM12 (http://www.fil.ion.ucl.ac.uk/spm/software/spm12/) and the Conn toolbox (Whitfield-Gabrieli & Nieto-Castanon, 2012) version 16b. Preprocessing of functional images included realignment, unwarping and slice-time correction, segmentation of gray-matter, white matter, and cerebrospinal fluid (CSF) and normalization to the MNI template. The data were additionally spatially smoothed with a Gaussian kernel set at 8 mm full width at half maximum. Signals from the segmented white matter and CSF, and the six motion realignment parameters and their first-order derivatives were regressed out of the signal. We have additionally regressed out outlier volumes (and the single volumes preceding the outliers) detected using the ART-based scrubbing method (based on a threshold of 2 mm subject motion and a global signal threshold of Z = 9). Subsequently, the data were linearly detrended and band-pass filtered (0.01 to 0.1 Hz). Two-levels of analysis were included. On the first level of analysis, seed-to-voxel maps were computed for each
subject based on individually localized seeds in each subject’s location of stimulation, where a spherical seed (6 mm radius) was defined using MarsBaR (marsbar.sourceforge.net). Individualized seed localization was done in 19/20 of the subjects. In one additional subject, storage of stimulation location was not saved due to technical malfunction. In this subject, the lPFC seed was based on the average lPFC coordinates of all other subjects. The maps express the correlation (Fisher Z-transformed Pearson’s correlation values) of each voxel with the mean time series extracted from each seed region of interest. Then, on the second level of analysis, the maps were subjected to a random effects second-level general linear model analysis, testing how connectivity correlated with a continuous covariate that expressed stimulation-dependent learning gains. The covariate was defined as learning gains following IPFC stimulation (data accumulating exactly on the line indicate equal learning gains in both IPFC and control stimulation). (c) Mean maximal learning gains following IPFC and control stimulation. Dashed lines reflect the percentage of participants on each side of the unit slope line in (b) and the bars reflect the mean maximal learning gains at each session. Error bars represent SEM included in the model as well. A voxel-level threshold of \( p < .001 \) was used in all analyses, qFDR (<0.05) corrected for multiple comparisons at the cluster level.

3 | RESULTS

3.1 | Effects of stimulation on learning

Our first objective was to probe for the role of human PFC in successful reinforced skill formation. We fitted the data with a Repeated measures ANOVA, with stimulation type (IPFC vs. control) and performance (baseline vs. peak) as within-subject factors. There was a significant main effect for performance \( (F_{1,19} = 233.916, p < .001; \eta_p^2 = 0.925) \), and a nonsignificant main effect for stimulation type \( (F_{1,19} = 0.325, p = .575; \eta_p^2 = 0.017) \). The interaction between the two factors was statistically significant \( (F_{1,19} = 4.505, p = .047, \eta_p^2 = 0.192) \). The interaction between the two factors was statistically significant \( (F_{1,19} = 4.505, p = .047, \eta_p^2 = 0.192) \); see Figure 2c; for single-subject data see Figure 2b), showing that maximal gains in performance were reduced following IPFC stimulation. These results suggest that in comparison to control stimulation, 1 Hz rTMS applied over the IPFC decreased reinforced skill learning gains (Figure 2c).
To rule out effects on motor performance per se (rather than learning), a control analysis showed that the differences between the prestimulation trial (baseline) and initial poststimulation trial (always unrewarded) were comparable across lPFC and control locations ($t_{19} = -0.49$, $p = .63$, Cohen’s $d = 0.109$, two-tailed). In addition, performance at the baseline trials, which were completed prior to the stimulation on each session, did not differ between the times of sessions ($t_{19} = 1.836$, $p = .082$, $d = 0.41$, two-tailed).

### 3.2 Association between baseline functional connectivity and stimulation effects

In light of lPFC’s dense functional connections with sensorimotor and reward networks (Cieslik et al., 2012; Haber, 2011; Hasan et al., 2013; Jarbo & Verstynen, 2015; Preston & Eichenbaum, 2013), we next tested if the effects of stimulation on learning gains were mediated by baseline functional connectivity with the lPFC, as recorded prior to the main stimulation/training sessions.

We first defined, for each of the subjects, intrinsic functional networks based on functional connectivity between the right IPFC and the rest of the brain. This network was primarily composed of clusters in contralateral lateral, orbitofrontal and dorsomedial PFC, and supramarginal and angular gyri (Supporting Information Figure S1), largely mirroring the widely studied frontoparietal control network (Vincent, Kahn, Snyder, Raichle, & Buckner, 2008). To assess how stimulation-dependent learning gains related to connectivity, we subjected the data to an analysis of covariance (ANCOVA) analysis (Figure 3b,c and Table 1). Stimulation-dependent learning gains correlated with functional connectivity between IPFC and sensorimotor cortex (mainly the medial and dorsolateral parts of the precentral gyrus), postcentral and central opercular cortex, and occipitotemporal cortex (Figure 3). There were no significant hippocampal or striatal clusters where functional connectivity correlated with learning gains.

### 3.3 Association between functional connectivity and gains in rewarded and unrewarded trials

Our behavioral paradigm alternated between rewarded and unrewarded trials, in a within-subject design. We thus next tested if stimulation-dependent learning gains differed in rewarded and unrewarded trials and how these two learning gain metrics related to IPFC functional connectivity (Figure 4a). The difference between stimulation-dependent gains in rewarded and unrewarded trials was not statistically significant ($t_{19} = -0.415$, $p = .683$, $d = -0.093$, two-tailed). The results however suggest a dissociation between these two learning metrics and IPFC functional connectivity. First, stimulation-dependent gains in rewarded trials were associated across subjects with connectivity between the lPFC and sensorimotor cortex, whereas no such association was found for unrewarded trials.

**TABLE 1** Functional connectivity and its relation to learning gains

<table>
<thead>
<tr>
<th>Cluster X Y Z</th>
<th>Locations</th>
<th>Cluster size</th>
<th>Cluster q-FDR</th>
<th>Peak p</th>
</tr>
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<td>14 36 70</td>
<td>PreCG (LR), PostCG (LR)</td>
<td>2552</td>
<td>.000001</td>
<td>.000004</td>
</tr>
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<td>48 14</td>
<td>PO (R), IC (R)</td>
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<td>.000002</td>
</tr>
<tr>
<td>50 16 18</td>
<td>CO (L), IC (L)</td>
<td>214</td>
<td>.004288</td>
<td>.000002</td>
</tr>
<tr>
<td>64 10 34</td>
<td>CO (R), PostCG (R)</td>
<td>191</td>
<td>.005785</td>
<td>.000063</td>
</tr>
<tr>
<td>52 62 70</td>
<td>iLOC (R), toMTG (R)</td>
<td>180</td>
<td>.006179</td>
<td>.000033</td>
</tr>
</tbody>
</table>

Clusters where functional connectivity correlated significantly with stimulation-dependent learning gains. MNI coordinates are shown for each cluster, along with its size, corrected FDR (q-FDR) and peak voxel-level $p$ value. CO = central Opercular cortex; IC = insular cortex; iLOC = inferior lateral occipital cortex; PO = parietal operculum; PreCG = precentral gyrus; toMTG = temporoparietal middle temporal gyrus.
postcentral and central opercular cortex and occipitotemporal cortex (Figure 4b). This pattern of connectivity was highly overlapping with that observed for stimulation-dependent gains, irrespective of reinforcement (as reported in Figure 3). Conversely, stimulation-dependent gains in unrewarded trials were associated with connectivity between lPFC and angular gyrus, extending to tempororooccipital Middle Temporal Gyrus (Table 2), with little overlap with the network that correlated with stimulation-dependent gains.

3.4 | Analysis of a control network

The results suggest a link between intrinsic lPFC functional connectivity and stimulation dependent learning gains. To test the specificity of these results, we examined the extent to which stimulation-dependent learning gains correlated with intrinsic connectivity in networks that do not implicate lPFC. To that extent, we localized the sensorimotor network (Biswal, Zerrin Yetkin, Haughton, & Hyde, 1995) in each of our subjects, based on seed region in right precentral gyrus (Supporting Information Figure S2). Connectivity in the resulting network did not significantly correlate with stimulation-related learning gains, suggesting that the results above were indeed specific to lPFC functional connectivity.

4 | DISCUSSION

Experimental support for the role of PFC and its functional interactions in learning keep accumulating (e.g., Antzoulatos & Miller, 2014; Neubert, Mars, Sallet, & Rushworth, 2015; Qin et al., 2014). While earlier studies have examined the causal role of PFC in value-based decision making (Smittenaar, FitzGerald, Romei, Wright, & Dolan, 2013) or in the context of implicit sequence learning (Galea, Albert, Ditye, & Miall, 2010), it remained incompletely understood how PFC and related networks are controlled in the human brain to support the acquisition of complex reinforced motor skills. Here, we designed a study to probe for the role of human PFC in successful reinforcement-based skill formation and examine how its interactions with functional large-scale networks contribute to skill acquisition. Our results show that a transient perturbation of lPFC significantly diminished learning gains, indicating a causal modulation of skill formation. Furthermore, we show that lPFC-dependent learning gains related specifically to the strength of intrinsic interactions between IPFC and sensorimotor regions. We further report that connectivity between IPFC and sensorimotor regions was primarily related to learning gains in rewarded trials. Altogether, the results suggest that
reinforced skill learning relies on IFPC and is related to the strength of functional interactions between IFPC and sensorimotor cortex.

Rather than solely through a local perturbation of IFPC activity, our results may suggest that IFPC stimulation affects reinforced skill learning through a distributed mechanism of operation. Distributed effects of rTMS have been extensively discussed in the literature (Chou et al., 2015; Dayan et al., 2013; Lee, Siebner, & Bestmann, 2006). Here, we show that pre-task intrinsic connectivity, recorded before stimulation, correlated with the effects of stimulation. Similar relations between baseline connectivity and later effects of stimulation were reported before. For example, markers based on intrinsic connectivity can predict the responsiveness of patients with depression to rTMS therapy (Drysdale et al., 2016; Salomons et al., 2014). Our results join these previous studies in suggesting that intrinsic functional connectivity (van den Heuvel & Hulshoff Pol, 2010), can predict the effects of stimulation, plausibly as stimulation itself affects distributed rather localized neural systems. In this respect, the combination of rTMS with assessment of intrinsic brain connectivity relates to other recent developments in noninvasive brain stimulation approaches, particularly methods allowing for simultaneous assessment of oscillatory brain activity during frontal brain stimulation (Chander et al., 2016; Witkowski et al., 2016) or closed-loop TMS paradigms (Zrenner, Belardinelli, Müller-Dahlhaus, & Ziemann, 2016). Utilization of such methods, in particular simultaneous imaging and stimulation methods will allow to more directly examine the distributed mechanism of operation underlying the local perturbation of brain regions. Future studies should also consider anatomical and functional markers of IFPC and aim to co-localize them with neuronavigation. This would encompass taking into account that F3/F4 stimulation based on the international 10–20 system may also engage frontal structures such as the frontal eye fields, implicated in processing spatial cues which may play a subsidiary role in sequence learning (Herwig et al., 2003).

Our results demonstrate that functional connections between the IFPC and sensorimotor regions were associated with stimulation-dependent learning gains. Reciprocal connections between IFPC and ventromedial PFC (Saraiva & Marshall, 2015), and between the more dorsal parts of IFPC and the frontal pole to rostral orbitofrontal cortex (Haber & Behrens, 2014) underlie motivated value-based processes. The contribution of the dorsal parts of IFPC to procedural learning (Dayan & Cohen, 2011) and executive motor behavior (Cieslik et al., 2012) has also been well-established. Transient perturbation of dorsolateral PFC via rTMS disrupts performance in an implicit sequence learning task, performed with the contralateral hand (Pascual-Leone et al., 1996). Moreover, it has been suggested that in the context of implicit sequence learning, dorsolateral PFC contributes specifically to the retention and manipulation of spatial information pertinent to the performance of the task (Robertson et al., 2001). Similarly, a meta-analysis of finger-tapping neuroimaging studies has found more pronounced involvement of lateral PFC in self-paced designs, relative to cued designs (Witt et al., 2008). As self-paced tapping tasks are likely more cognitively demanding, the involvement of lateral PFC in several sequence learning tasks may reflect heightened recruitment of cognitive control centers in the brain (Witt et al., 2008).

Interestingly, IFPC (specifically, the superior frontal gyrus) is among a set of hub regions which are not only more densely structurally connected to other regions in the brain but are also densely connected among themselves. This so called "rich club" organization, demonstrated in both human (Grayson et al., 2014; van den Heuvel & Sporns, 2011) and non-human brains (Liang et al., 2017) is believed to allow information integration within large-scale brain systems, and may allow memory and reward systems to interact during motor skill learning.

Several recent studies have established that procedural and motor learning are mediated by reinforcement, whether in the form of reward or punishment (Abé et al., 2011; Dayan, Averbeck, et al., 2014; Galea, Mallia, Rothwell, & Diedrichsen, 2015). While only a few studies have sought to identify the neural substrates underlying reward based motor and procedural learning, our results fit in well with previous data, suggesting that the IFPC mediates the efficacy of reward during skill learning (Dayan, Hamann et al., 2014). More generally, through its connections with orbital and medial PFC, the IFPC plays a pivotal role in value-based learning (Dixon & Christoff, 2014) and has been linked primarily with anticipation of reward (Bjork & Hommer, 2007) and the representation of motivationally relevant outcomes (Dixon & Christoff, 2014; Liu, Hairston, Schrier, & Fan, 2011). While our results suggest that connectivity between IFPC and sensorimotor regions was primarily related to learning gains in rewarded trials, they cannot be taken as reflecting a strict difference between rewarded and unrewarded trials. As in our paradigm learning alternated stochastically between rewarded and unrewarded trials (Dayan, Averbeck, et al., 2014; Dayan, Hamann et al., 2014), it is plausible to assume that subjects acted under incentive motivation also in unrewarded trials. Paradigms that separate rewarded and unrewarded trials between subjects are needed to further explore the association between reward-based learning and intrinsic interactions in large-scale brain networks.

It has been suggested that motor skill learning likely relies on both striatal-procedural and hippocampal-declarative systems (Stanley & Krakauer, 2013). While the current results did not implicate fronto-hippocampal connectivity in the effects of IFPC stimulation on learning gains, it would be of interest to test the role of declarative knowledge formation in future studies, using suitable tasks. Future work could test for memory and reward system interaction using declarative tasks which have a weaker motor component, or alternatively using interference paradigms that assess interactions among the two systems (Brown & Robertson, 2007a, 2007b).

In sum, we report here that perturbation of IFPC significantly reduced subjects’ reinforced learning gains, and further show that these effects were related to the strength of task-free functional connectivity in intrinsic connections between IFPC and sensorimotor cortex. Our results thus suggest that IFPC may contribute to incentive-based acquisition of procedural skills through its interactions with the sensorimotor system. As such, our results support a systems-level characterization of this form of learning.

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CONFLICT OF INTEREST
The authors have no Conflicts of Interest to disclose.

ORCID
Eran Dayan http://orcid.org/0000-0001-9710-9210
Nitzan Censor http://orcid.org/0000-0001-7608-6064

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**SUPPORTING INFORMATION**

Additional supporting information may be found online in the Supporting Information section at the end of the article.

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